



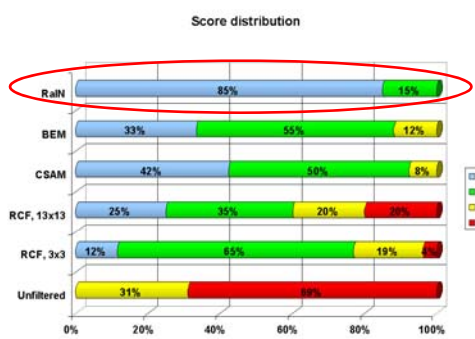
Impulsive noise: results

- 156 images images unfiltered / treated with the proposed filter / with other impulsive noise filters;
- 15 experts for evaluation;
- Scores:
 - 0 => image with no pulses
 - 1 => no more than two pulses identified in no more than two analyzed areas
 - 2 => many (>2) pulses visible in a few (≤ 2) areas of the image or few pulses (≤ 2 pulses) visible in several (>2) areas of the image (> 2)
 - 3 => more than 2 pulses were visible in many (>2) areas of the image.



Impulsive noise: results

- How many pixels are modified by the filter?





Filter	Score 0	Score 1	Score 2	Score 3
RaIn	85%	15%	0%	0%
BEM	33%	55%	12%	0%
CSAM	42%	50%	8%	0%
RCF, 13x13	25%	35%	20%	20%
RCF, 3x3	12%	65%	19%	4%
Unfiltered	0%	0%	31%	69%

- Prop. method: 0.14%
- BEM: 0.80%
- CSAM: 1.67%
- RCF 13x13: 0.23%
- RCF 3x3: 4.73%



Impulsive noise removal: summary

- Mixture of noise: an accurate description of the statistical properties of the noise to accurately classify the pulses;
- Less pixels modified by the filter, but...
- ... Less pulses left on the image.

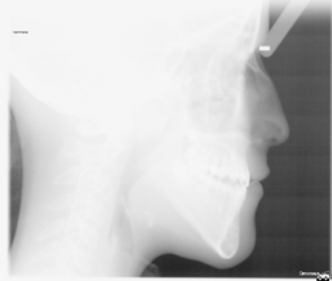




Overview


- Statistical models and digital radiography
- Impulsive noise removal filter
- Soft tissue filter
- Conclusion

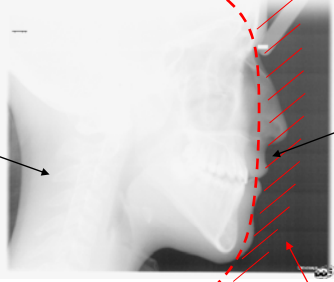
Soft tissue filter: exposure issue


- Underexposed radiographies: bone cannot be distinguished from soft tissue
- Overexposed radiographies: soft tissue tends to mix with background
- In any case, soft and bone tissue are hard to be optimally exposed at the same time.
- Digital radiographies are acquired on 12 bpp, displayed at 8 bpp.



Soft tissue filter: exposure issue



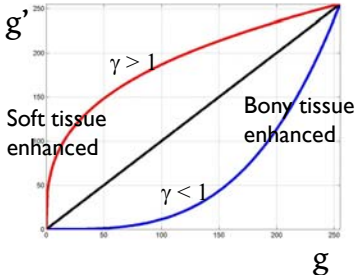
- A raw solution, not so effective..




Soft tissue filter: γ correction

- Gray level correction (NB images are negative images, white = low signal);
- Used for global exposure correction;
- For 8 bit image, gray level g is corrected to g' as:


$$g' = 255 \cdot [(g / 255)^{1/\gamma}]$$




$\gamma > 1 \rightarrow$ Stretching of the low levels, compression of the high levels.
 $\gamma < 1 \rightarrow$ Compression of the low levels, stretching of the high levels.




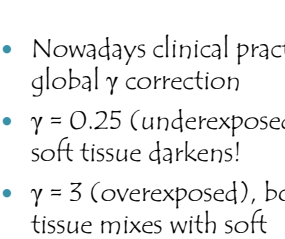
Soft tissue filter: γ correction




$\gamma = 3$









$\gamma = 0.25$






- Nowadays clinical practice: global γ correction
- $\gamma = 0.25$ (underexposed), soft tissue darkens!
- $\gamma = 3$ (overexposed), bone tissue mixes with soft tissue!



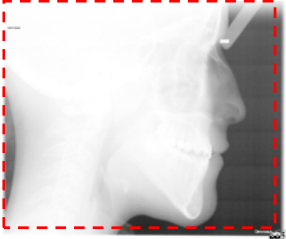
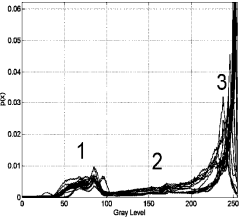
Soft tissue filter: the idea

(I. Frosio and N.A. Borghese, IEEE Trans. Med. Imag. 2006)


- Exposure issue: different γ for bony and soft tissue;
- An adaptive γ correction scheme has to be identified;
- How to modulate the value of γ across the image?
- (soft) image clusterization through mixture model



Soft tissue filter: Typical histogram

- Three characteristic gray zones: background (1), soft tissue (2), bone tissue (3)
- 5% boundary eliminated (white margins, logo)
- Black pixels are eliminated (saturated pixels)




Soft tissue filter: the mixture

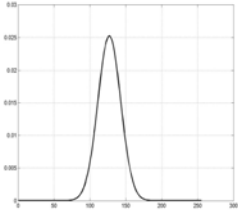
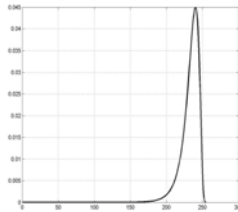
- Mixture model: a linear combination of M probability density functions:

$$p_{MM}(x) = \sum_{j=1}^M P(j) \cdot p(x | j)$$


- The most common mixture: mixture of Gaussians.



Soft tissue filter: the mixture

- Mixture of three components ($M = 3$)
- Two Gaussians: background, soft tissue (symmetric peaks)
- One Inverted Lognormal: bone tissue (asymmetric peak)




Soft tissue filter: EM

- **Parameters:** $P(j)$ – mixing parameters and μ_j, σ_j for each distribution: $j=1\dots 3$
- $n = 1:N$, number of pixels
- Negative log likelihood:

$$E = -\ln L = -\sum_{n=1}^N \ln p_{MM}(x^n) = -\sum_{n=1}^N \ln \{p(x^n | j)P(j)\}$$

- E is minimized with respect to the parameters through the EM algorithm

$$p_{MM}(x) = \sum_{j=1}^M P(j) \cdot p(x | j)$$




Soft tissue filter: EM

Histogram
↓


- Mixing parameters: $P(j)^{new} = \frac{1}{N} \sum_{g=0}^{N_{GL}-1} P^{old}(j|g) \cdot H(g)$
- Gaussians:

$$\mu_j^{new} = \frac{\sum_{g=0}^{N_{GL}-1} P^{old}(j|g) \cdot g \cdot H(g)}{\sum_{g=0}^{N_{GL}-1} P^{old}(j|g) \cdot H(g)} \quad (\sigma_j^{new})^2 = \frac{\sum_{g=0}^{N_{GL}-1} P^{old}(j|g) \cdot (g - \mu_j^{new})^2 \cdot H(g)}{\sum_{g=0}^{N_{GL}-1} P^{old}(j|g) \cdot H(g)}$$
- Lognormal:

$$\mu_j^{new} = \frac{\sum_{g=0}^{N_{GL}-1} P^{old}(j|g) \cdot \ln(N_{GL} - g) \cdot H(g)}{\sum_{g=0}^{N_{GL}-1} P^{old}(j|g) \cdot H(g)} \quad (\sigma_j^{new})^2 = \frac{\sum_{g=0}^{N_{GL}-1} P^{old}(j|g) \cdot [\ln(N_{GL} - g) - \mu_j^{new}]^2 \cdot H(g)}{\sum_{g=0}^{N_{GL}-1} P^{old}(j|g) \cdot H(g)}$$




Soft tissue filter: hard segmentation

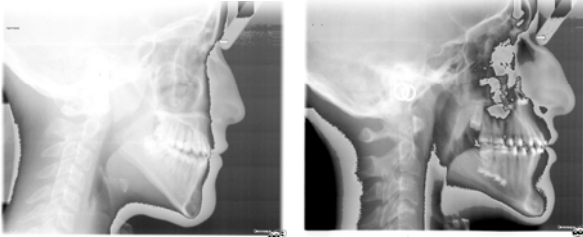


- Threshold $Th(j, j+1)$ minimizes


$$\int_0^{Th(j, j+1)} P(j+1) \cdot p(x | j+1) dx + \int_{Th(j, j+1)}^{N_{GL}-1} P(j) \cdot p(x | j) dx$$
- Three classes: Background, soft tissue, bone tissue



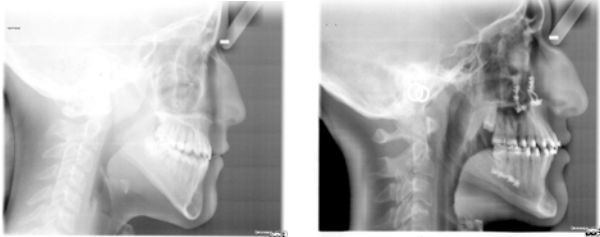
Soft tissue filter: hard segmentation



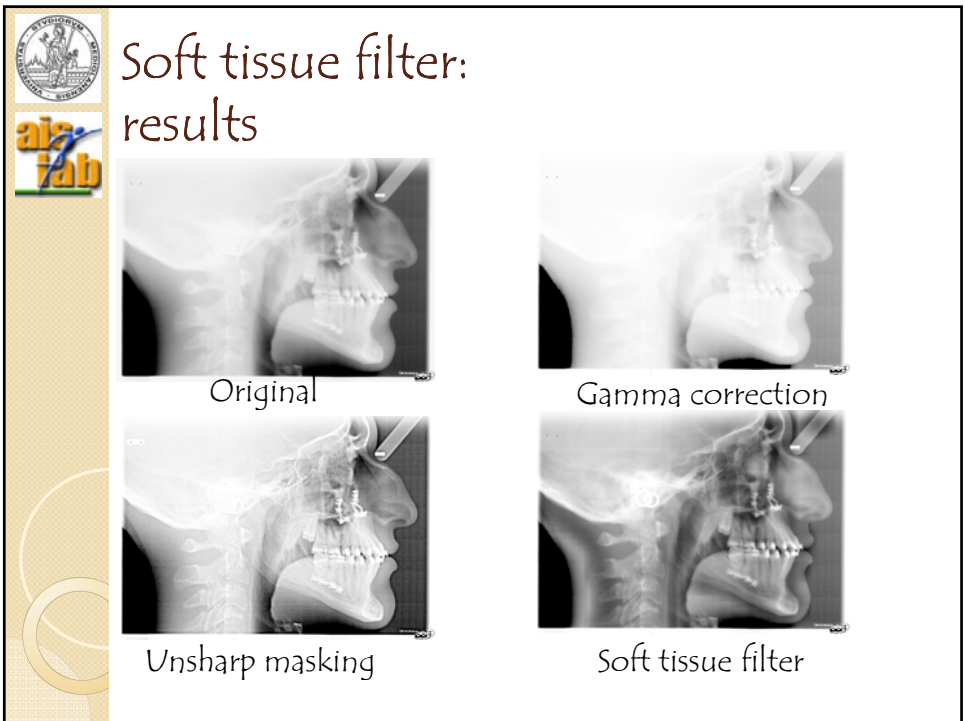
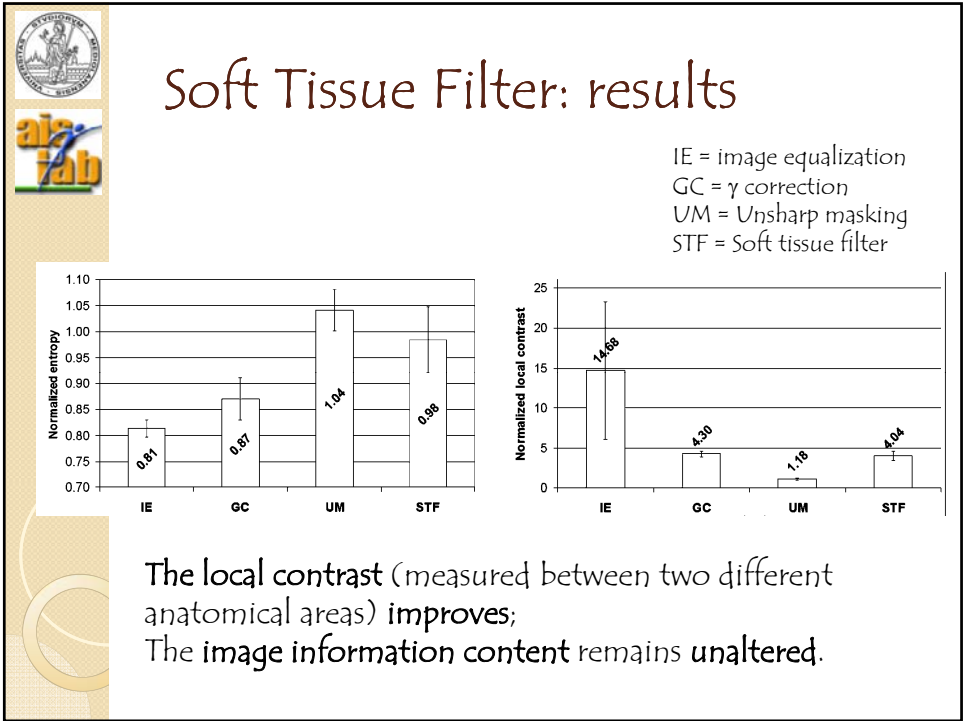
- $\gamma = 1$ background
- $\gamma = 0.25$ bone tissue
- $\gamma = 1.5$ soft tissue
- Artifacts, patient profile not clearly visible!




Soft tissue filter: soft segmentation




- γ map has to be smoothed
- Down sampling, moving average 3×3 filtering, up sampling using bilinear interpolation (or efficient moving average filter in space domain)
- Two classes: Background & soft tissue, bone tissue





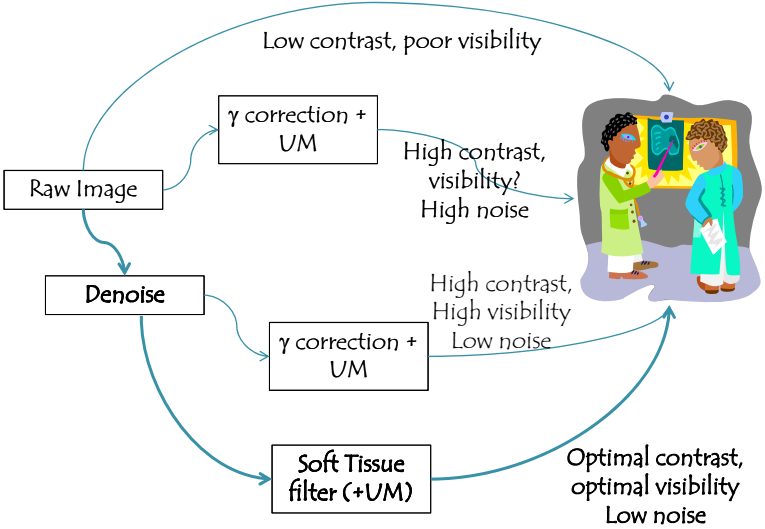
Overview

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- Impulsive noise removal filter
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- Conclusion



Impulsive noise removal + soft tissue filter

N. A. Borghese, I. Frosio (2010). Denoising and Contrast Enhancement in Dental Radiography. Handbook of Research on Dental Computing and Applications, Ed. A.Daskalaki.



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graph TD; RawImage[Raw Image] --> UC[Low contrast, poor visibility]; RawImage --> Denoise[Denoise]; Denoise --> UC; Denoise --> UC2[High contrast, High visibility Low noise]; Denoise --> UC3[Optimal contrast, optimal visibility Low noise]; UC --> UC4[High contrast, visibility? High noise]; UC2 --> UC4; UC3 --> UC4; UC4 --> UC; UC4 --> UC2; UC4 --> UC3;
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The flowchart illustrates the process of dental radiography image enhancement. It starts with a 'Raw Image' which has 'Low contrast, poor visibility'. This image can be processed in three ways: 1) Directly to 'High contrast, visibility? High noise' via γ correction + UM. 2) Through a 'Denoise' step to 'High contrast, High visibility Low noise' via γ correction + UM. 3) Through a 'Denoise' step to 'Optimal contrast, optimal visibility Low noise' via a 'Soft Tissue filter (+UM)'. The 'High contrast, visibility? High noise' path leads to a doctor and patient examining a screen, which then feeds back into the 'Low contrast, poor visibility' state. The 'High contrast, High visibility Low noise' and 'Optimal contrast, optimal visibility Low noise' paths also lead to the doctor and patient, and they both feed back into the 'High contrast, visibility? High noise' state.



Conclusion

- **Principled statistical models** as an effective alternative to traditional filtering;
- Computational demand is no more an issue. Technology advance promise even faster computation (e.g. CUDA);
- Accurate description of the image statistical properties leads to "optimal" filters (in a likelihood sense);
- Better statistical models can be considered?



References

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